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## Description

### Background of the Invention

[0001] The present invention is directed to emitting biofluids from drop ejection units, and more particularly to priming mechanisms used to obtain proper drop ejection sensing and controlling the level of biofluid within drop ejection devices.

[0002] Various designs have been proposed for the ejection of biofluids which permit the high-speed printing of sequences and arrays of drops of biofluids to be used in various tests and experiments. In the present discussion, a biofluid, also called a reagent, may be any substance used in a chemical reaction to detect, measure, examine or produce other substances, or is the substance which is to be detected, measured, or examined.

[0003] Biofluid ejection devices find particular utility in the depositing of drops on to a substrate in the form of a biological assay. For example, in current biological testing for genetic defects and other biochemical aberrations, thousands of the individual biofluids are placed on a glass substrate at different well-defined locations. Thereafter, additional depositing fluids may be deposited on the same locations. This printed biological assay is then scanned with a laser in order to observe changes in the biofluid property.

[0004] It is critical in these situations that the drop ejection device not be a source of contamination or permit unintended cross-contamination between different biofluids. Also, due to the high cost of these biofluids, and the importance of positioning properly formed drops at highly precise locations, it is important that the drop ejectors operate correctly at the start of the drop ejection process.

[0005] In view of the foregoing, it has been considered desirable to provide priming mechanisms which ensure the proper delivery of biofluids to an ejector device in a timely, useful manner.

### Summary of the Invention

[0006] Provided is a priming mechanism for priming a biofluid drop ejection device having a drop ejection opening leading to an ejection reservoir. The priming mechanism includes a vacuum unit which generates a vacuum force, connected to a vacuum nozzle. The vacuum nozzle is located over the drop ejection opening. A disposable sleeve or tubing is attached to the vacuum nozzle and is placed in operational contact with the drop ejection opening. A fluid height detection sensor is positioned to sense a fluid height within at least one of the disposable tubing and the vacuum nozzle. Upon sensing a predetermined fluid height, by the fluid height detection sensor, the priming operation is completed, and the primer mechanism is removed from the operational contact with the drop ejection opening.

[0007] In a further embodiment the opening is an

opening to a priming reservoir.

[0008] In a further embodiment the vacuum unit is controlled to provide a variable vacuum force.

### Brief Description of the Drawings

[0009]

FIGURE 1 illustrates an acoustic drop ejection unit with which the present invention may be implemented;

FIGURES 2A and 2B depict fluid levels in a reagent cartridge;

FIGURE 3 sets forth a laser biofluid level detection mechanism;

FIGURES 4A and 4B depict an acoustic beam biofluid level detector configuration;

FIGURE 5 illustrates a drop-counting detection mechanism;

FIGURE 6 sets forth a first embodiment for movement of a reagent cartridge in a two-piece acoustic drop ejection unit;

FIGURE 7 shows a second embodiment of a supplemental supply for a two-piece acoustic drop ejection mechanism;

FIGURE 8 sets forth a single piece acoustic drop ejection mechanism within which the concepts of the present invention may be implemented;

FIGURE 9 depicts a first embodiment for supplying additional biofluid in a single-piece system;

FIGURE 10 sets forth a second embodiment for a one-piece acoustic drop ejection mechanism;

FIGURE 11 depicts a second embodiment for a single-piece acoustic drop ejection mechanism;

FIGURE 12 illustrates a single piece piezo-electric drop ejection mechanism having a secondary biofluid holding region;

FIGURE 13 depicts a two-piece piezo-electric drop ejection mechanism having a secondary biofluid holding region;

FIGURE 14 sets forth a priming configuration for a piezo-electric drop ejection mechanism; and

FIGURE 15 illustrates a modified single piece piezoelectric drop ejection mechanism incorporating a priming reservoir.

### Detailed Description of Preferred Embodiments

[0010] FIGURE 1 is a cross-sectional view of an acoustic drop ejection unit 10, having a reagent cartridge 12 inserted within an acoustic drop ejection mechanism 14. A transducer 16 is supplied with energy by a power supply source 18. Transducer 16 is provided on a surface of substrate 20, such as glass. Patterned or located on an opposite surface of glass substrate 20 is a focusing lens configuration 22, such as a Fresnel lens. It is to be appreciated that other types of focusing configurations may also be used in place of Fresnel lens 22.

[0011] A connecting layer 24, such as an acoustic coupling fluid is located between Fresnel lens 22 and reagent cartridge 12. The acoustic coupling fluid 24 is selected to have low acoustic attenuation. An example of an acoustic coupling fluid having beneficial acoustic characteristics for this application include water. In an alternative embodiment connecting layer 24 may be provided as a thin layer of grease. The grease connection will be useful when the joining surfaces are relatively flat in order to minimize the possibility of trapped bubbles.

[0012] On top of glass substrate 20 are walls 26, 28 which define interior chamber 30 within which reagent cartridge 12 is located. Side wall 31 of cartridge 12 includes a seal 32 extending from its outer surface. Seal 32 secures cartridge 12 within chamber 30 and maintains acoustic coupling fluid 24 below seal 32. A precision depth stop 34 holds cartridge 12 at a desired insertion location. A thin membrane 36 is formed on a lower surface 37 of cartridge 12, positioned substantially above Fresnel lens 22. Membrane 36 is an acoustically thin membrane, wherein acoustically thin is defined in this context to mean that the thickness of the membrane is small enough that it passes over 50% of its incident acoustic energy through to biofluid 38 within cartridge 12.

[0013] In operation, energization of transducer 16 emits an acoustic wave which travels through glass substrate 20 to Fresnel lens 22. The lens produces a focused acoustic energy wave 39 that passes through acoustic coupling fluid 24 and membrane 36, reaching an apex at biofluid meniscus surface 40 of biofluid 38. Supplying of the focused energy to surface 40 causes disruptions in the surface resulting in ejection of a biofluid drop 42 from cartridge 12 to substrate 43, such as paper, glass, plastic or other appropriate material. The biofluid ejected can be as small as approximately 15µm in diameter. However, this size limitation is based on the physical components used, and it is to be understood that drops ejected by an acoustic drop ejection unit can be made smaller or larger in accordance with design changes to the physical components.

[0014] The surface from which biofluid drops 42 are ejected can be either totally open or contained by an aperture plate or lid 44. The lid 44 will have a suitably sized aperture 45, which is larger than the ejected drop size in order to avoid any interference with drop ejection. Aperture 45 must be sized so that the surface tension of meniscus 40 across aperture 45 sufficiently exceeds the gravitational force on biofluid 38. This design will prevent biofluid 38 from falling from reagent cartridge 12 when cartridge 12 is turned with aperture 45 facing down. The aperture down configuration has a benefit of maintaining the biofluid 38 clean from material which may fall from substrate 43.

[0015] Operation of transducer 16, power supply 18, glass substrate 20, and lens 22 function in a manner similar to previously discussed drop ejection units used

in the field of acoustic ink printing. Such operation is well known in the art.

[0016] The foregoing design isolates biofluid 38 within reagent cartridge 12, preventing it from coming into contact with drop ejection mechanism 14, or other potential sources of contamination, such as airborne contamination or contamination from biofluids previously used with the ejection mechanism. Reagent cartridge 12 is separated from acoustic coupling fluid 24 by membrane 36. The entire cartridge may be injection molded from a biologically inert material, such as polyethylene or polypropylene. Cartridge 12 is operationally linked to the acoustic drop emitter mechanism 14 by a connection interface which includes membrane 36 and acoustic coupling fluid 24.

[0017] In a specific design of the present invention, the width of reagent cartridge 12 may be approximately 300 microns, and membrane 36 may be 3 microns thick. In this particular embodiment, with a design constraint of a focal acoustic wave length being 300 microns and at an operating frequency of known acoustic drop ejection mechanisms, the meniscus location should be maintained within plus or minus five microns from an ideal surface level.

[0018] Power supply source 18 is a controllably variable. By altering the output of power supply source 18, energy generated by transducer 16 is adjusted, which in turn may be used to alter the volume of an emitted biofluid drop 42.

[0019] As previously discussed, for proper operation of the acoustic drop ejection device 10, the location of the meniscus surface 40 must be maintained within tolerances defined by the device configuration. While in the previously discussed embodiment, due to the specific acoustic drop ejection mechanism being used, that tolerance is +/- 5 microns. It is to be appreciated other ranges exist for differently configured devices.

[0020] The concept of maintaining biofluid levels of a reagent cartridge 12 within a set level of parameters is illustrated by FIGURES 2A and 2B. For example, FIGURE 2A shows reagent cartridge 12 when it is full of biofluid 38. In FIGURE 2B the same cartridge 12 is shown in an empty state. It is to be appreciated that empty in this embodiment refers to there being less biofluid 38 than the predetermined parameter height 46, in this instance 10 microns. Thus, there is still biofluid within cartridge 12. However, due to the operational characteristics of acoustic drop ejection unit 10, once biofluid 38 is outside of the predetermined level 46 biofluid drops cannot be reliably ejected. This situation exists since the apex of acoustic wave 39 is not occurring at surface 40 of biofluid 38, and sufficient energy is not transferred to disturb the surface to the degree that a drop will be ejected at this lower level.

[0021] Thus, for useful operation of biofluid drop ejection unit 10, it is desirable to provide a configuration which detects the biofluid level while the cartridge 12 is within acoustic drop mechanism 14.

[0022] Turning to FIGURE 3, illustrated is a first embodiment of a biofluid level detection mechanism 50 which is capable of measuring the level of biofluid 38 within cartridge 12, when cartridge is within ejector mechanism 14.

[0023] As biofluid drops are ejected from cartridge 12, the level of biofluid 30 will change. Biofluid level detection mechanism 50 includes a laser 52 positioned such that laser beam 54 emitted therefrom is reflected off of the upper surface 56 of biofluid 38. A laser detection configuration 58 includes a first laser beam detector 60 and a second laser beam detector 62. First laser beam detector 60 is positioned at an angle relative to the acoustic drop ejection unit 10 such that when cartridge 12 has biofluid within the predetermined parameters, the angle of reflected laser beam 64 will impinge upon sensor 60. Laser beam detector 62 is positioned at an angle relative to acoustic drop ejection unit 10 such that it will sense reflected laser beam 66 which is at an angle corresponding to the biofluid 38 being out of the acceptable range for proper operation.

[0024] The outputs of sensor detector 60 and sensor detector 62 are provided to a controller 68. This information, along with preprogrammed information as to location of the laser 52 and detectors 60, 62, is used to calculate the biofluid level. The information obtained by controller 68 may then be used in further control of the biofluid level, as will be discussed in greater detail below.

[0025] Turning to FIGURES 4A and 4B, set forth is a second embodiment for level sensing in accordance with the present invention. Particularly, controller 70 controls the output of power supply 72 to initiate a short pulse acoustic wave 76 to be transmitted from Fresnel lens 78 to the upper surface 80 of biofluid 38. Controller 70 controls the output from power supply 72 such that short pulse acoustic wave 76 is not sufficient to cause the emission or ejection of a biofluid drop. Rather, short pulse acoustic wave 76 is emitted, and sensed by lens 22. This outbound acoustic wave 76, as shown in FIGURE 4A reaches surface 80 and is then reflected back 84 towards lens 22, generating an rf signal provided to controller 70 with an indication of the emission and return of acoustic wave 76.

[0026] The time taken for acoustic wave 76 to travel to surface 80 and back to lens 22 is used to determine whether the biofluid is at an appropriate level. This information will be used to adjust the fluid level, as will be discussed in further detail below. In an alternative embodiment, it is possible to vary the supplied frequency to shift the focus, in order to maintain the acoustic wave at the meniscus surface.

[0027] Controller 70 is designed to determine the time from emission of the outbound acoustic wave 76 until receipt of the reflected wave 84 having been preprogrammed with parameters as to the speed of the acoustic wave, the depth of the biofluid in cartridge 12 when full, the viscosity of the biofluid as well as other required

parameters. Using this information controller 70 calculates the biofluid level within cartridge 12. This information is then used in later level control designs which will be discussed in greater detail below.

5 [0028] In an alternative embodiment controller 70 may be designed to sense an amplitude of the returned wave. The sensed amplitude is correlated to the biofluid level. Particularly, the returned signal of acoustic wave 76 will carry with it amplitude information. If the fluid height is not at an appropriate level, either too high or too low, the amplitude will be lower than expected. The returned amplitude will be at a peak when the fluid is at a correct level for ejector operation. Therefore, to determine the proper level the volume of biofluid is altered and a measurement is made to determine if the returned amplitude is closer or further from maximum amplitude. Dependent upon whether fluid was added or removed and the reaction of the amplitude, it can be determined whether more or less biofluid is needed.

10 [0029] Turning to FIGURE 5, illustrated is a further embodiment of biofluid level detection in accordance with the present invention. Sound pulses emitted by lens 22 are supplied to controller 88. The controller 88 is configured to accumulate and count the pulses received, and to correlate that value to the known average volume of biofluid ejected in each drop. Controller 88 then inferentially calculates the level of biofluid 38 within cartridge 12. This biofluid level information is then used to control the biofluid level.

15 [0030] It is to be appreciated that while alternative embodiments for biofluid level detection in cartridge 12, have been disclosed in connection with FIGURES 3, 4A, 4B and 5, other configurations may also be implemented.

20 [0031] As previously mentioned, by altering the frequency of operation it is possible, using a Fresnel lens design, to alter the amplitude of the emitted acoustic wave. Using this capability the peak of the emitted acoustic wave is controllable. Therefore, as biofluid is emitted, but still within an acceptable range, the amplitude may be adjusted to properly sense the new surface level. By this design additional biofluid does not need to be added until a lower surface level is sensed.

25 [0032] Turning to FIGURE 6, illustrated is a first embodiment for altering the position of the reagent cartridge 12 located within the acoustic drop ejection mechanism 14. The position change is made in response to the detection of biofluid levels by techniques shown, for example, in connection with FIGURES 3, 4A, 4B or 5.

30 [0033] When the level of biofluid is determined to be out of a desired range, an adjustment to the level of the reagent cartridge 12 is undertaken. Particularly, provided is an auxiliary fluid chamber 90 placed in operational communication with chamber 30 via chamber connect 92. When it is determined the biofluid level is out of an acceptable range, additional acoustic connection fluid 94 is supplied to chamber 30 by activation of plunger 96. Plunger 96 may be a high-precision plunger control-

led by a computer-driven actuator 98. Computer-driven actuator 98 is provided with signals via any one of the controllers 68, 70 or 88 previously discussed in connection with FIGURES 3, 4A, 4B and 5. Plunger 96 is moved inward forcing supplementing acoustic connection fluid 94 into chamber 30 to raise reagent cartridge 12 to a sufficient amount to ensure that surface 80 is within the acceptable height range.

**[0034]** FIGURE 7 is a side view of a two piece drop ejection unit 100 employing an alternative reagent cartridge 102 configuration. In addition to ejection reservoir 104 which holds biofluid 38, a main reservoir 106 is also provided to feed ejection reservoir 104. A connection path between the ejection reservoir 104 and main reservoir 106 is provided via reservoir connect 108. In this design, as biofluid 38 is ejected from ejection reservoir 104, additional biofluid 38 is supplied via the main reservoir 106 and reservoir connect 108.

**[0035]** Reagent cartridge 102 is in operational arrangement with acoustic drop ejection mechanism 110. Ejection reservoir 104 is located over lens 22, glass substrate 20, and transducer 16 in a manner which allows generated acoustic energy to be focused, and transferred to the ejection reservoir 104 with sufficient energy to emit biofluid drops. In implementing this two piece design connecting layer 24, such as an acoustic coupling fluid is provided, and a bottom portion of cartridge 102 is formed with membrane 112 which allows sufficient acoustic energy to be transferred to ejection reservoir 104.

**[0036]** Main reservoir 106 is filled through filling port 114. The main reservoir 106 and reservoir connect 108 use capillary action to assist in an initial filling of the ejection reservoir 104 when it is in an empty state. Thereafter, as drops are ejected from ejection reservoir 104 surface tension causes biofluid from the main reservoir to be drawn into the ejection reservoir. Particularly, aperture 45 of ejection reservoir 104 is sufficiently sized smaller than filling port 111 of main reservoir 106 and also small enough to overcome gravitational forces due to reservoir height, that biofluid in main reservoir 106 is drawn into the ejection reservoir 104.

**[0037]** Turning to FIGURE 8, set forth is a single piece biofluid acoustic ejection unit 120. Distinctions between the two-piece biofluid drop ejection unit 10 and the single-piece unit 120, include that seal 32 of reagent cartridge 12 is no longer used. Rather, reagent cartridge 122 has side wall 124 with a planar external surface 126 in direct contact with walls 26,28 of mechanism 14. Therefore, a permanent connection is made between walls 26, 28 and reagent cartridge 122. Such connection may be made during the manufacture of the device via lithographic techniques and/or by use of known adhesion technology.

**[0038]** In a further embodiment, lower surface 128, including membrane 130, may be removed allowing biofluid 38 to come into direct contact with lens 22. Still a further embodiment is to remove cartridge 112 and sup-

ply the biofluid directly into chamber 30, where chamber 30 acts as a non-contaminated biofluid containment area. Under this design chamber 30 is filled with biofluid in a contamination-free environment.

**[0039]** FIGURE 9 shows an embodiment for supplying additional biofluid to reagent cartridge 140 in order to maintain the biofluid 38 at a desired level. In this embodiment auxiliary fluid holding area 142 has a bellows-shaped configuration with an interior 144 filled with biofluid 38.

**[0040]** Upon receipt of a signal from a level-sensing device (e.g. FIGURES 3, 4A, 4B and 5) indicating biofluid within ejection reservoir 146 is below a desired level, precision plunger 148, controlled by computer operated actuator 150, is moved inward compressing auxiliary biofluid holding chamber 142. This action forces a predetermined amount of biofluid 38 into main chamber 146 such that biofluid meniscus surface 152 is moved to an acceptable, usable level.

**[0041]** FIGURE 10 depicts a second embodiment for supplying additional biofluid 38 to reagent chamber 160. In this instance, collapsible auxiliary area or chamber 162 is in fluid communication with ejection reservoir 164. Upon receiving a level signal indicating the level of biofluid 38 is required to be replenished, squeezing mechanism 166 is activated by a computer-controlled actuator 168 to provide inward force on collapsible chamber 162. Pressure is applied in a sufficient amount to resupply ejection reservoir 164 with biofluid, to an acceptable usable level.

**[0042]** Turning to FIGURE 11, illustrated is an alternative embodiment for a single piece acoustic drop ejection unit 170. In this figure, ejection reservoir 172 and main reservoir 174 are placed in fluid communication by reservoir connect 176. Biofluid 38 is supplied from main reservoir 174 to ejection reservoir 172 due to surface tension at the meniscus, as discussed in connection with FIGURE 7. Transducer 16 is in operational connection to substrate 178 on a first surface 180, and lens 22 is on a second surface 182 whereby these components are formed as part of the single unit 170. In this embodiment, connecting layer 24 of FIGURE 7 is not required due to the single component disposable nature of the present embodiment. In ejection reservoir 172, biofluid comes into direct contact with lens 22. Therefore, there is no need for the acoustic coupling fluid provided in FIGURE 7. Main reservoir 174 is filled through filling port 183.

**[0043]** FIGURE 12 is a side view of a single piece piezoelectric drop ejection unit 190. Ejection reservoir 192 is connected to main reservoir 194 via reservoir connect 196. Biofluid is supplied to main reservoir 194 via filling port 198. A piezo actuator 200 is in operational attachment to a lower surface 202 of ejection reservoir 192. An upper surface defining the ejection reservoir 192 has formed therein an ejection nozzle 204.

**[0044]** In operation piezo actuator 200 is actuated by power supply 210, which in combination with lower sur-

face 202, define a unimorph, and deflects in response to an applied voltage. In this instance a force is imposed such that the unimorph configuration moves into ejection reservoir 192, thereby altering the volume of ejection reservoir 192, which in turn forces biofluid from the ejection reservoir 202 through nozzle 204 as an ejected biodrop. The size of nozzle 204 is a controlling factor as to the size of the ejected drops.

[0045] As biofluid drops are emitted from ejection reservoir 192, surface tension in the ejection reservoir causes biofluid located in main reservoir 194 to be drawn through reservoir connect 196 into ejection reservoir 192, thereby replenishing the biofluid level. In the present embodiment, main reservoir 194 has an internal dimension of 1 cm in length and 2.5 mm in height. The width of the overall piezoelectric drop ejection unit is 5 mm. In one embodiment the volume of biofluid in a full main reservoir may be from 50 to 150 microliters and the biofluid in the ejection reservoir may be between 5 and 25 microliters. The ratio of biofluid in the reservoirs may range from 2 to 1 up to 10 to 1. In other situations the ratio may be greater. The volume of biofluid drops may be in the picoliter range.

[0046] As can be seen in FIGURE 12, lower surface 202 connected to piezo actuator 200 is integrated into the overall piezoelectric drop ejector unit 190. Under this construction, when biofluid of unit 190 is depleted, the entire unit 190 may be disposed.

[0047] Turning to FIGURE 13, illustrated is a side view of a two piece piezoelectric biofluid drop ejection unit 220 having a disposable portion and a reusable portion. The disposable portion includes a main reservoir 222 and an ejection reservoir 224 which has integrated therein an ejection nozzle 226. The ejection reservoir 226, being connected to main reservoir 222 via reservoir connect 230. Transmission of biofluid from main reservoir 222 to ejection reservoir 226, via reservoir connect 230 occurs due to surface tension existing in ejection reservoir 224. Also included is a filling port 232.

[0048] The reusable portion of unit 220 includes piezo actuator 240 powered by a power supply source 234. The piezo actuator 240 is carried on a reusable frame 244.

[0049] A lower surface of ejection reservoir 224 is formed as a membrane 246 and is connected to an upper surface or diaphragm 248 of reusable frame 244. Diaphragm 248 is bonded or otherwise connected to piezo actuator 240 such that diaphragm 248 acts as part of a unimorph structure to create a necessary volume change within ejection reservoir 226 in order to eject a biofluid drop from ejection nozzle 224. Membrane 246 of cartridge 222 acts to transfer the volume change in the reusable portion 244 into the disposable portion.

[0050] In a further embodiment, the reusable portion has a flexible membrane with a piezo actuator on one surface to generate the volume displacement necessary to expel a biofluid drop. A container may be fabricated to place a connecting liquid in contact with the transducer/membrane.

This liquid assists in transmitting the transducer-induced volume changes to a second membrane on a different container surface. The container edges are constructed to make a hermetic seal between the reusable and the disposable parts. The container has a provision for removing (bleeding) air bubbles from the connecting liquid. The opposite surface is open before assembling with the disposable part.

[0051] A hermetic seal is provided between the disposable and reusable portions, and the reusable portion is filled with a connecting liquid to transmit the volume changes from the transducer to the disposable portion. To minimize compliance and absorption of volume changes, all air bubbles in this fluid are removed before operation by bleeding them through a bleeding mechanism in the reusable portion.

[0052] One skilled in the art would understand that other piezo actuator configurations, such as bulk or shear mode designs, may also be used in conjunction with the present invention.

[0053] In the foregoing discussion, configurations are disclosed which function to ensure that the necessary biofluid levels are maintained in a system. In an alternative embodiment, the concepts discussed in connection with FIGURES 4A and 4B may be used in systems where additional biofluid is not added.

[0054] In one embodiment an adjustment of the generated acoustic wave is used to extend the operational capabilities of the system. This embodiment is applicable to both a Fresnel lens and a spherical lens.

[0055] With attention to FIGURES 4A and 4B, rather than using controller 70 to selectively activate an actuator, controller 70 supplies signal generator 12 with an indication to increase or decrease amplitude output when it is determined that the fluid height is not at the desired level. By this action, the focal point of the acoustic wave is adjusted to occur at the actual meniscus height.

[0056] A further embodiment would be to again use the concepts of FIGURES 4A and 4B to detect that the fluid height is not at a desired level. Thereafter, when using a Fresnel lens, it is possible to change operational frequency in order to tune the focal point to the exact fluid height existing at a particular time within the device. For a Fresnel lens the focal position is substantially a linear function of frequency. Therefore, in FIGURES 4A and 4B, the initial step is measurement of the actual biofluid level. Then, controller 70 tunes the frequency of operation such that the focal point is moved to where the meniscus surface actually exists.

[0057] Using the foregoing design, it is possible to present a system which forgoes the use of an actuator. Rather, use of frequency control and/or amplitude control expands the range of the appropriate biofluid level for operation of the device. For example, without amplitude or frequency control described above, the range for appropriate use would be  $\pm 5$  microns from an ideal level. However, by implementing amplitude control this

can be expanded to potentially +/- 10 microns, and through frequency control to +/- 30 microns.

[0058] The frequency and acoustic control concepts may be used alone, without the use of an actuator, or in connection with actuator concepts to provide a more refined control.

[0059] In piezoelectric drop ejection units, initial operation may not produce desired drop output. Particularly, when air bubbles exist within the ejection reservoir, non-spherical drops, or drops which are not of a proper consistency or size may be ejected, and more likely no drops will be produced. Therefore, a priming of the ejection unit is desirable.

[0060] FIGURE 14 illustrates a primer connection or mechanism 250 which may be used in accordance with the present invention. As shown in FIGURE 14, the primer connection 250 is located over a nozzle (204, 226) which is configured to emit biofluid from an ejection reservoir (192, 224). In operation, disposable primer connection 250 may be a robotically actuated device which moves over an ejection nozzle (204, 226). The primer connection 250 includes a permanent vacuum nozzle 252 connected to a vacuum unit 254. Placed around permanent vacuum nozzle 252 is a disposable tubing or sleeve 256 made of an elastomeric or other suitable material. Once located over ejection nozzle (204, 224), the vacuum nozzle 252 is moved downward, placing the disposable tubing 256 into a loose contact with nozzle (204, 226). Vacuuming action vacuums air out of the ejection reservoir (204, 226).

[0061] A robotically controlled fluid or liquid height detection sensor 258 determines when the biofluid has reached a level, such that air within the ejection reservoir has been removed. This priming operation permits for proper initial drop ejection operation. Once the detector 258 has sensed an appropriate priming level has been reached, the priming operation is ended by removal of the priming mechanism from operational attachment with the drop ejection unit.

[0062] Robotically controlled primer connection 250 and liquid height detection sensor 258 may be controlled by a controller 259. Controller 259 generates actuation signals controlling movement of these robotically controlled elements. It is to be appreciated that detection sensor 258 may in fact be integrated as part of the primer connection 250. Movement of primer connection 250 and detection sensor 258 may be accomplished by one of many known configurations, and the mechanical components necessary for such movement are well known in the art.

[0063] In an alternative embodiment, the primer connection 250 and level detector 258 may themselves be stationary and it is the drop ejection unit which is moved appropriately underneath the primer connection 250. In either case, it is to be understood that primer connection 250 and level detector 258 represent a multiple number of such configurations to prime an array of drop ejector units in a single drop ejector head. Similarly, the embod-

iment which will be discussed in connection with FIGURE 15 is also representative of such an array of components.

[0064] Once a priming operation has been undertaken for a particular drop ejection unit, disposable tubing 256 may be replaced prior to a next priming operation.

[0065] It is noted that vacuum unit 254, controlled by controller 259 is capable of generating a controllable vacuum force which causes the vacuuming action previously described. By having the controllable force, adjustments dependent upon the viscosity of the biofluid can be taken into account. For example, a larger vacuum force may be applied for a biofluid with greater viscosity than a biofluid which is more liquid. It is noted that vacuum nozzle 252 has been defined as permanent. By this discussion, permanent is intended to mean permanent compared to the disposable tubing 256. However, it is to be understood that in other embodiments, the connection between the vacuum unit 254 and vacuum nozzle 252 may have detachable characteristics. For example, the vacuum nozzle may be attached by a snap-fit connection, a set screw or other connection technique which allows for removal of the nozzle.

[0066] Turning to FIGURE 15, illustrated is a modified single piece piezoelectric drop ejection unit 260 designed in a manner similar to the ejection unit 190 illustrated in FIGURE 12. Therefore common elements are numbered similarly. However, the presently configured unit 260 also includes a priming reservoir 262 having a priming opening 264. Priming is accomplished by movement of priming system 250 to a position over priming opening 264. Once sleeve 256 is engaged with opening 264, a vacuum pressure is applied to draw the biofluid for priming purposes. During this operation, power supply 210 generates pulses for activation of piezo actuator 200 in order to move biofluid within ejection reservoir 192 up to nozzle 204.

[0067] It is to be understood that the reagent cartridges discussed in the foregoing embodiments are simply representative designs of such a device, and that there are many possible variations to the cartridge configuration.

[0068] While the foregoing description sets forth embodiments for acoustic drop ejection units and piezoelectric drop ejection units, the concepts of the present invention may be extended to other drop ejection mechanisms and for fluid other than biofluids for which avoidance of contamination is beneficial.

## Claims

1. A priming mechanism for priming a biofluid drop ejection unit having an opening, the priming mechanism comprising:

a vacuum unit which generates a vacuum force;  
a vacuum nozzle connected to the vacuum unit,



the vacuum nozzle is located over the opening of the drop ejection unit;  
a tubing attached to the vacuum nozzle, and in operational contact with the opening of the drop ejection unit; and  
a fluid height detection sensor positioned to sense a fluid height within at least one of the disposable tubing and vacuum nozzle.

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2. The invention according to claim 1 further including a controller which controls movement and operation of at least one of the vacuum unit and fluid height detection sensor. 10
3. The invention according to claim 1 wherein the priming mechanism is robotically controlled. 15
4. The invention according to claim 1 wherein once the fluid height detection sensor detects fluid at a predetermined height, a priming operation is ended and the priming mechanism is removed from the operational contact with the drop ejection device. 20
5. The invention according to claim 1 wherein the tubing is disposable. 25
6. The invention according to claim 1 wherein the vacuum unit, the vacuum nozzle and the fluid height detection sensor are configured as a single element. 30
7. The invention according to claim 1 wherein the priming mechanism is movable and is moved over a stationary drop ejection unit. 35
8. The invention according to claim 1 wherein the priming mechanism is stationary and the drop ejection unit is movable, and is moved beneath the priming mechanism. 40
9. The invention according to claim 1 wherein the drop ejection unit is a piezoelectric drop ejection unit. 45
10. The invention according to claim 9 wherein the opening is a nozzle of the piezoelectric drop ejection unit. 50

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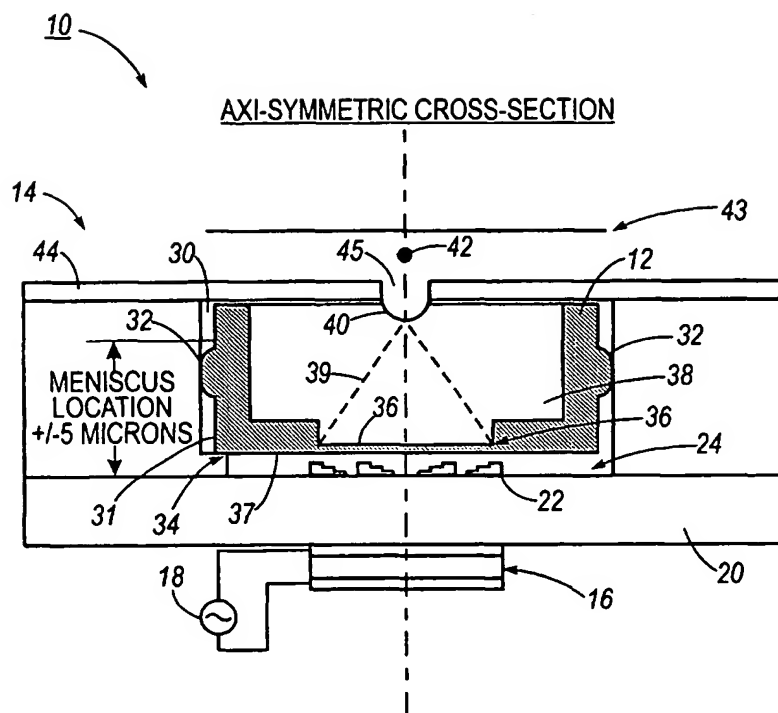
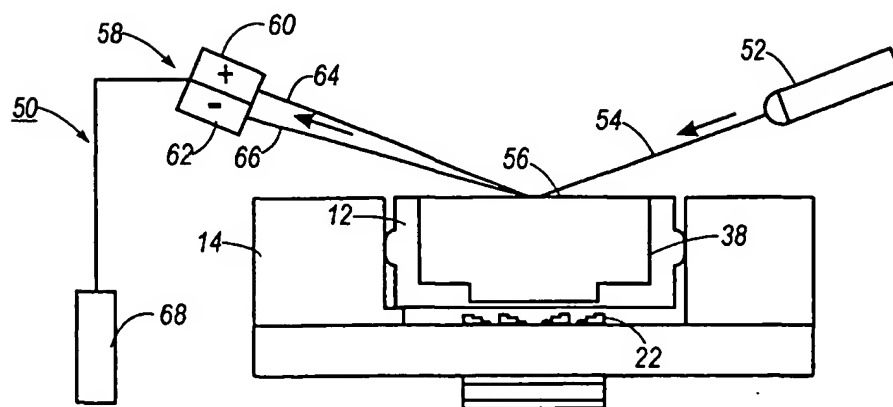
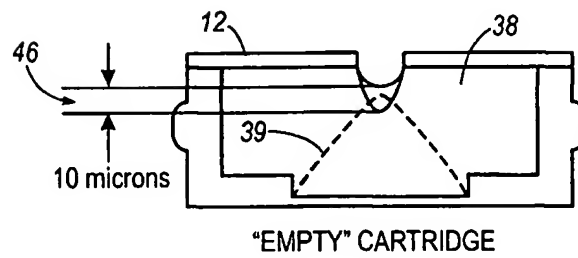
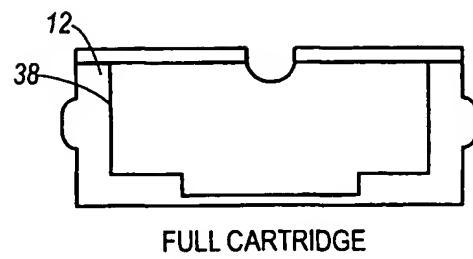


FIG. 1



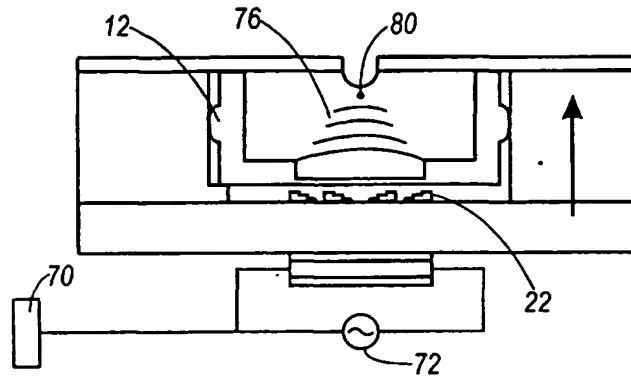


FIG. 4A

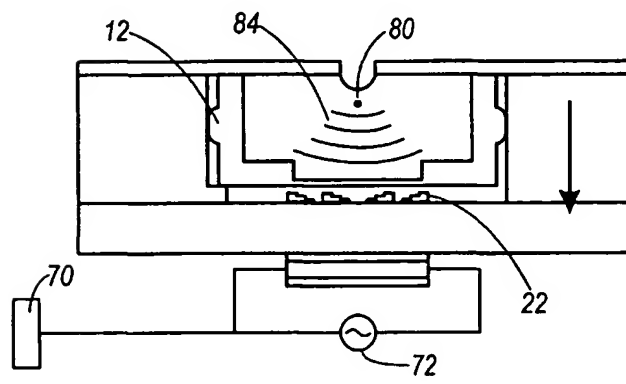


FIG. 4B

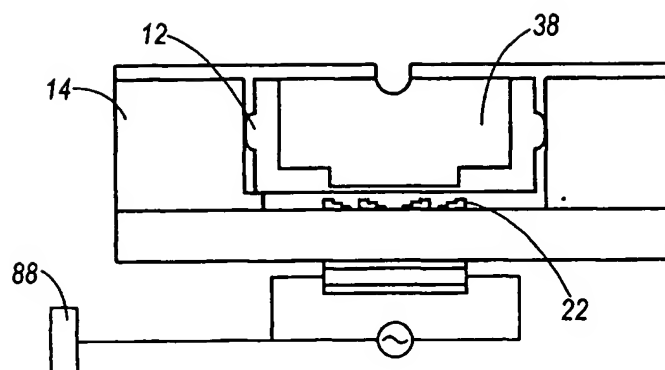


FIG. 5

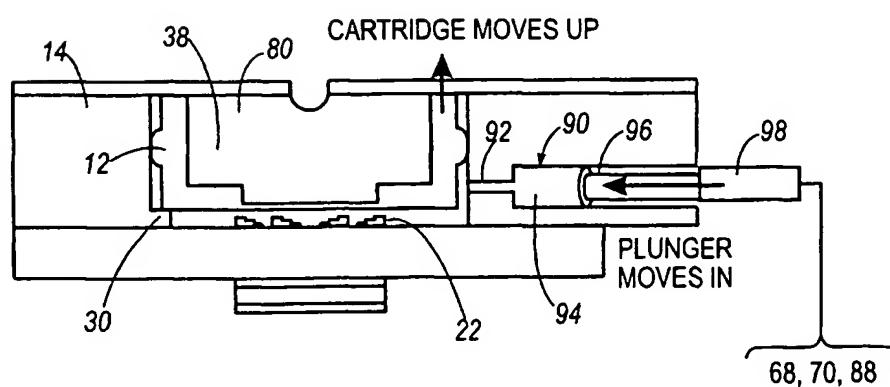
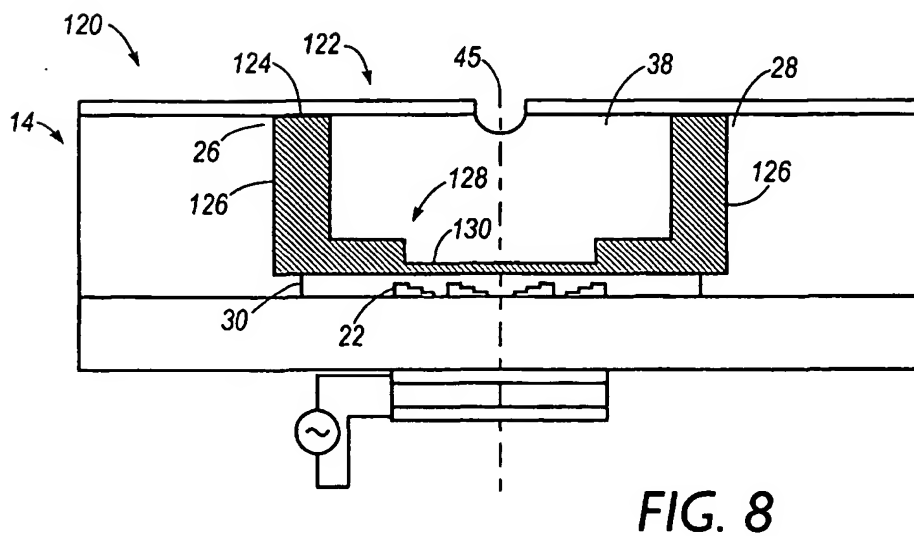
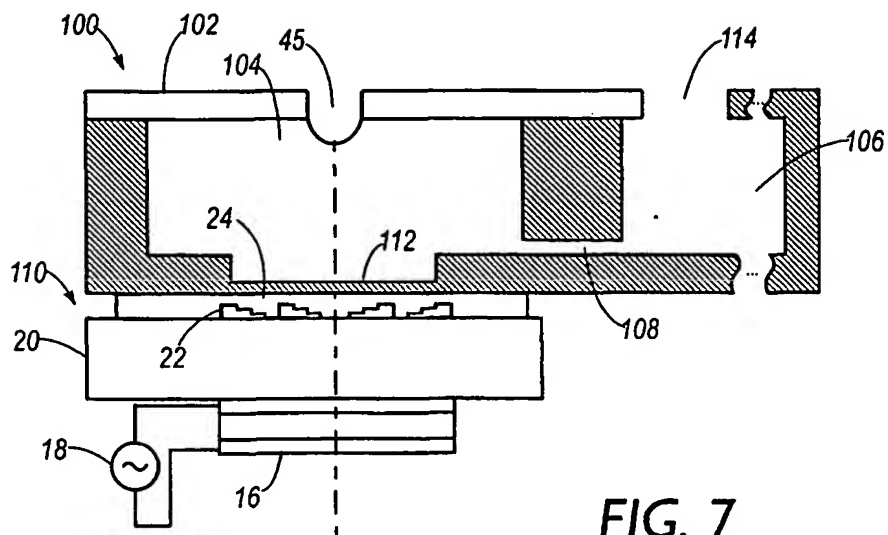


FIG. 6



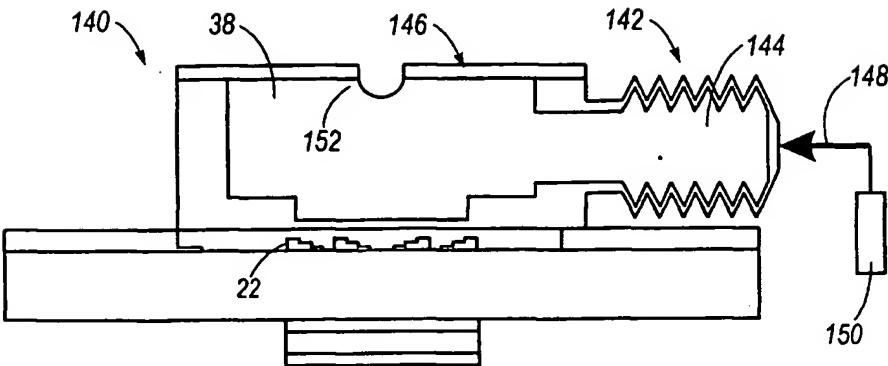


FIG. 9

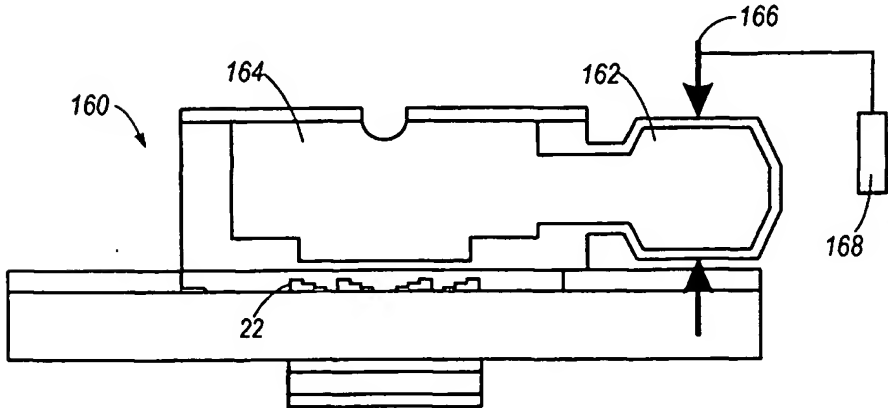


FIG. 10

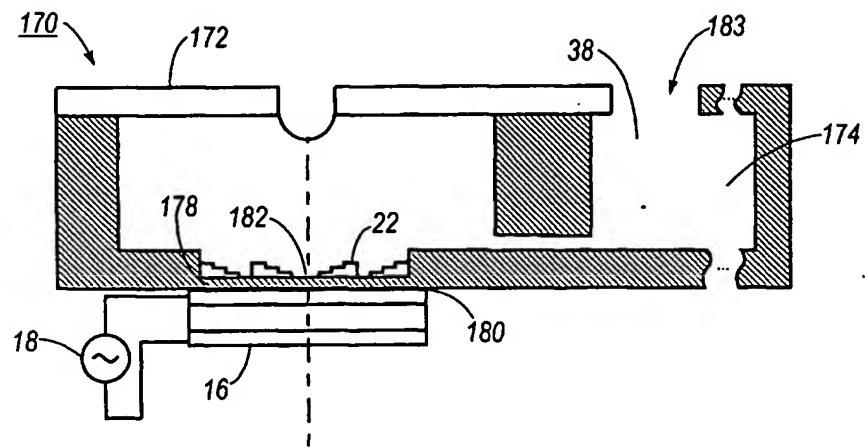


FIG. 11

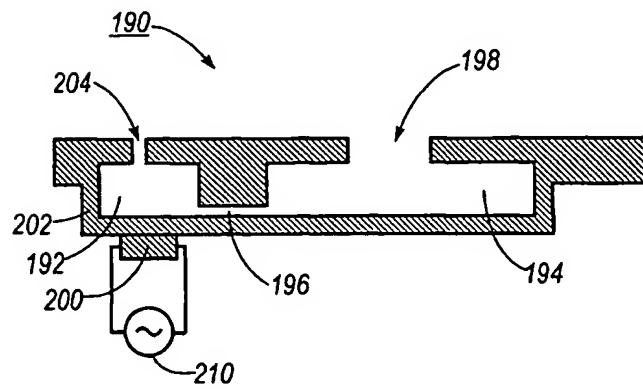


FIG. 12



FIG. 13

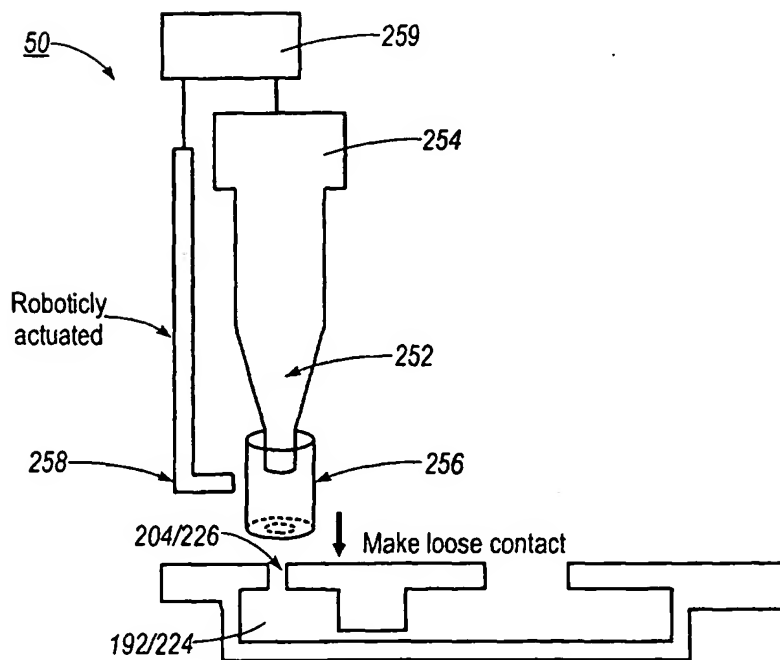
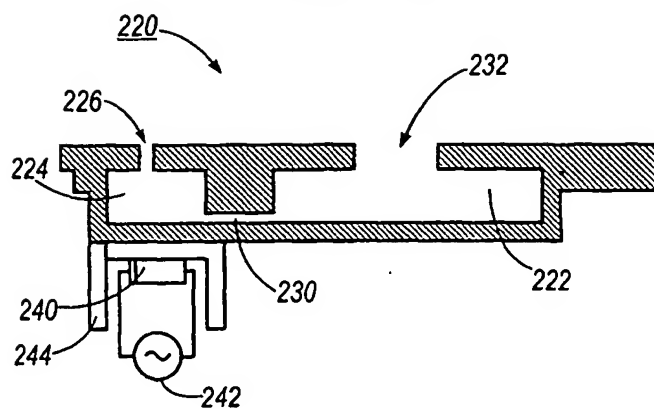


FIG. 14

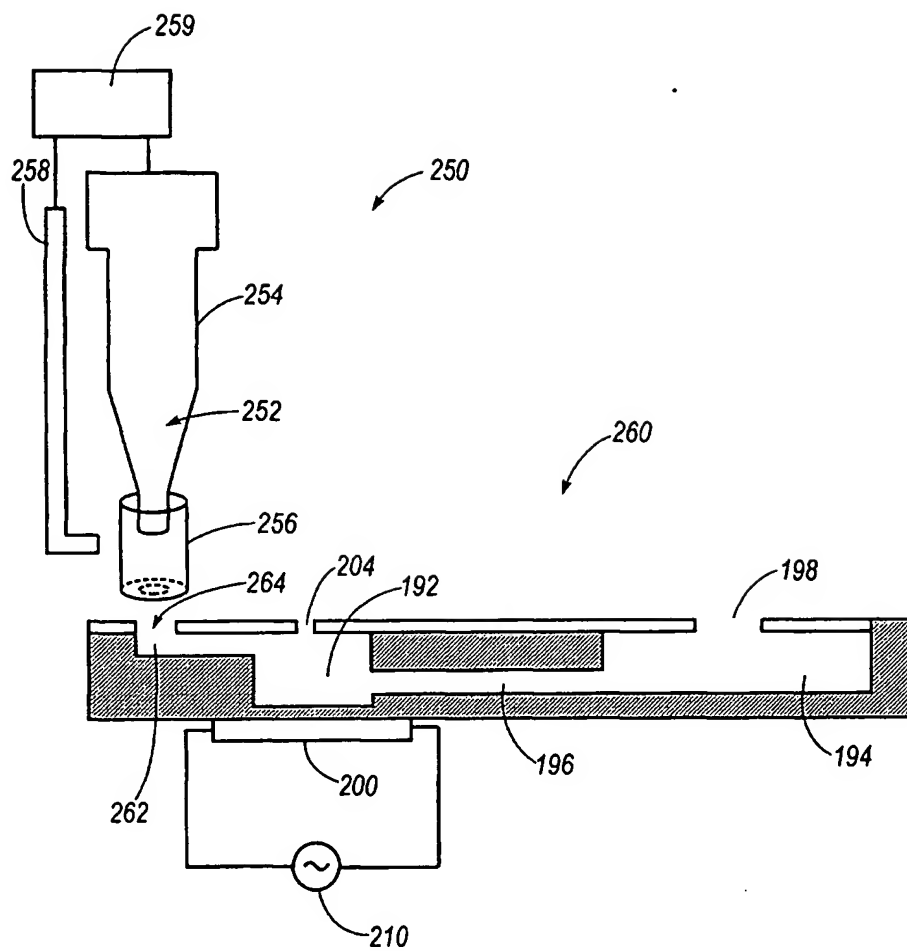


FIG. 15